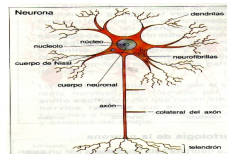
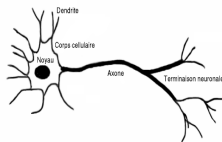


# PDEs for neural networks analysis, simulations and behaviour

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Centro Ennio De Giorgi, sept. 2017



- I. The single neuron,
  - I. 1. Excitable systems
  - I. 2. slow-fast dynamics,
  - I. 3. Integrate&Fire model, role of noise
  
- II. Networks, I&F
  
- III. Networks, time elapsed models

Electrically active cells are described by an **action potential**  $V(t)$

Models are well established

■ Hodgkin-Huxley

■ FitzHugh-Nagumo

■ Morris-Lecar

■ Mitchell-Schaeffer

$$\begin{aligned}C \frac{dv}{dt} &= I - g_{Na} m^3 h (V - V_{Na}) - g_K n^4 (V - V_K) - g_L (V - V_L) \\ \frac{dm}{dt} &= a_m(V)(1-m) - b_m(V)m \\ \frac{dh}{dt} &= a_h(V)(1-h) - b_h(V)h \\ \frac{dn}{dt} &= a_n(V)(1-n) - b_n(V)n \\ a_m(V) &= .1(V+40)/(1-\exp(-(V+40)/10)) \\ b_m(V) &= 4 \exp(-(V+65)/18) \\ a_h(V) &= .07 \exp(-(V+65)/20) \\ b_h(V) &= 1/(1+\exp(-(V+35)/10)) \\ a_n(V) &= .01(V+55)/(1-\exp(-(V+55)/10)) \\ b_n(V) &= .125 \exp(-(V+65)/80)\end{aligned}$$

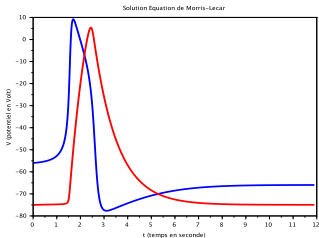
The class of Morris-Lecar is typically

$$\begin{cases} \frac{dV(t)}{dt} = \sum_{i=1}^I g_i(t)(V_i - V(t)) + I(t), \\ \frac{dg_i(t)}{dt} = \frac{G_i(V(t)) - g_i(t)}{\tau_i}, \quad g_i(0) \geq 0, \quad i = 1, 2, \dots, I, \end{cases}$$

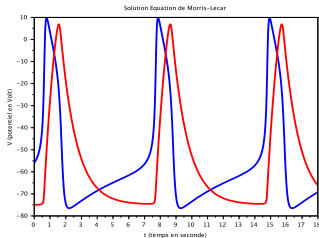
- The index  $i$  refers to ionic channels along the nerve (Ca, K, Na, Cl...)
- The  $V_i$  are called the “reversal potentials” (Nernst-Planck theory)
- The leak  $V_L$  is used to aggregate some of them
- $\tau_i$  can be  $\ll 1$
- Sharp nonlinearities  $G_i$  (sigmoids)

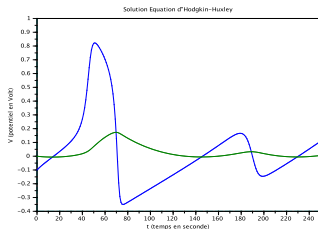
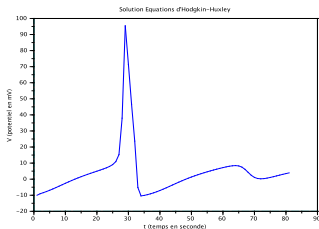
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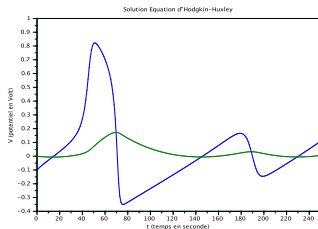
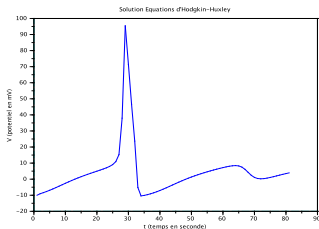
Hyperpolarization





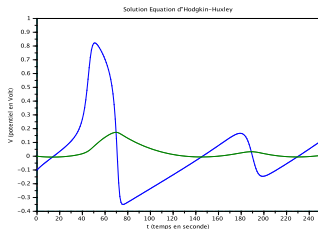
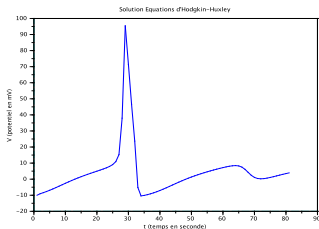
Solutions of Hodgkin-Huxley's model and of FitzHugh-Nagumo's model

- these models are accurate
- represent the property of **excitability** and **hyperpolarization**



Solutions of Hodgkin-Huxley's model and of FitzHugh-Nagumo's model

- these models are accurate
- represent the property of **excitability**
  - A small perturbation generates a large trajectory
  - Return to equilibrium
  - The trajectory depends very little on the perturbation



Solutions of Hodgkin-Huxley's model and of FitzHugh-Nagumo's model

- These models are accurate BUT
- difficult to understand why they are **excitable**
- expensive for large assemblies of neurones
- do not explain properties of large assemblies
- This motivates using simpler models



FitzHugh-Nagumo

$$\begin{cases} \varepsilon \dot{v}(t) = f(v(t)) - w(t), & v(t=0) = v^0, \\ \dot{w}(t) = v(t) - v^* - \alpha w(t) & w(t=0) = w^0. \end{cases}$$

It can be derived from the Morris-Lecar model

$$\begin{cases} \frac{dV(t)}{dt} = g_L(V_L - V(t)) + G_{Na}(V(t))(V_{Na} - V(t)) + g_K(t)(V_K - V(t)) \\ \frac{dg_K(t)}{dt} = \frac{G_K(V(t)) - g_K(t)}{\tau_K} \end{cases}$$

$$V_K < V_L < V_{Na}$$

FitzHugh-Nagumo

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$$v(t) = \ln(V(t) - V_K)$$

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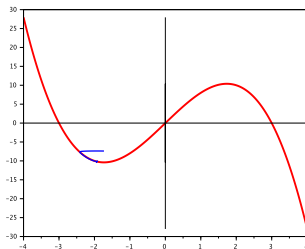
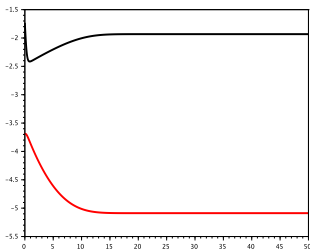
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$$\frac{dv(t)}{dt} = \underbrace{\frac{g_L(V_L - V(t)) + G_{Na}(V(t))(V_{Na} - V(t))}{V(t) - V_K}}_{:=F(v(t))} - g_K(t)$$

## FitzHugh-Nagumo

$$\begin{cases} \varepsilon \dot{v}(t) = f(v(t)) - w(t), \\ \dot{w}(t) = v(t) - v^* \end{cases} \quad \begin{cases} v(t=0) = v^0, \\ w(t=0) = w^0. \end{cases}$$

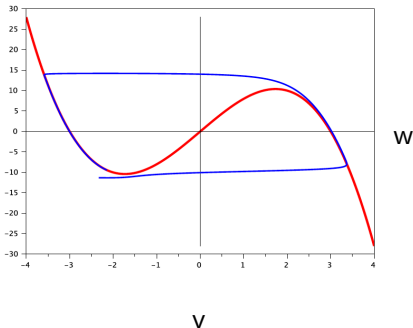
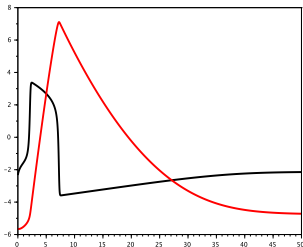


$w$

$v$

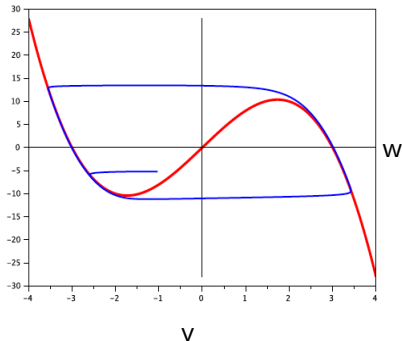
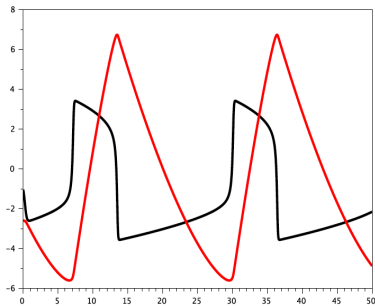
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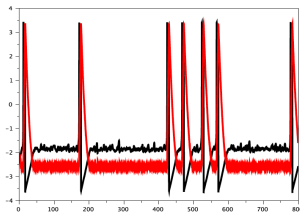
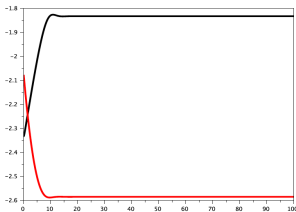


## FitzHugh-Nagumo

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# Single neuron : Role of noise



$$\begin{cases} \frac{dv(t)}{dt} = f(v(t)) - w(t), \\ \frac{dw(t)}{dt} = v(t) - v^* + \frac{dB(t)}{dt}. \end{cases}$$

Slow-fast dynamics

$$\begin{cases} \varepsilon \dot{v}_\varepsilon(t) = f(v_\varepsilon(t)) - w_\varepsilon(t), & v_\varepsilon(t=0) = v^0, \\ \dot{w}_\varepsilon(t) = v_\varepsilon(t) - v^* & w_\varepsilon(t=0) = w^0. \end{cases}$$

**Theorem** As  $\varepsilon \rightarrow 0$ , we have

- $v_\varepsilon(t) \rightarrow v$  a.e.,
  - $w_\varepsilon(t) \rightarrow w(t)$  uniformly (locally)
- and

$$\frac{dw(t)}{dt} = Q_\pm(w(t)) - v^*, \quad v(t) = Q_\pm(w(t))$$



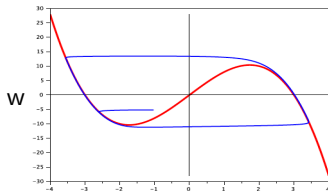
Slow-fast dynamics

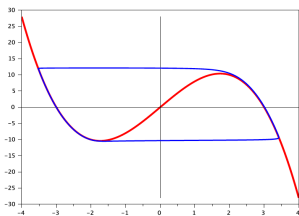
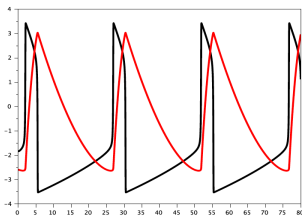
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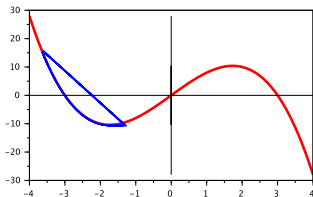
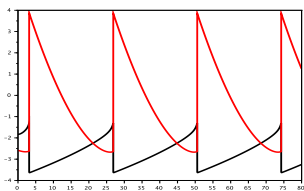
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(FitzHugh-Nagumo, fast discharge) solution of a variant of the FitzHugh-Nagumo system

$$\begin{cases} \frac{dv(t)}{dt} = h(v(t)) + I(t), & \tau_i \leq t < \tau_{i+1}, \\ v(\tau_i) = V_R, & \lim_{t \rightarrow \tau_{i+1}^-} v(t) = v(\tau_{i+1}) = V_F. \end{cases}$$



Solution of the integrate-and-fire system

- Single neurone models are numerous and complex
- They share the property to describe excitability
- The I&F model is derived has a double Slow-Fast limit
- The I&F model simply describes the discharge at a determined threshold